

**HIGH REFRACTIVE INDEX
POLYMERIC SILOXYSILANE COMPOSITIONS**

Field of the Invention:

[0001] The present invention relates to monomers useful in the manufacture of biocompatible medical devices. More particularly, the present invention relates to siloxysilane monomers capable of polymerization or copolymerization to form polymeric compositions having desirable physical characteristics for use in the manufacture of ophthalmic devices.

INNOVATION DOCUMENT

Background of the Invention:

[0002] Since the 1940's ophthalmic devices in the form of intraocular lens (IOL) implants have been utilized as replacements for diseased or damaged natural ocular lenses. In most cases, an IOL is implanted within an eye at the time of surgically removing the diseased or damaged natural lens, such as for example, in the case of cataracts. For decades, the preferred material for fabricating such IOL implants was poly(methyl methacrylate) (PMMA), which is a rigid, glassy polymer.

[0003] Softer, more flexible IOL implants have gained in popularity in more recent years due to their ability to be compressed, folded, rolled or otherwise deformed. Such softer IOL implants may be deformed prior to insertion thereof through an incision in the cornea of an eye. Following insertion of the IOL in an eye, the IOL returns to its original pre-deformed shape due to the memory characteristics of the soft material. Softer, more flexible IOL implants as just described may be implanted into an eye through an incision that is much smaller, i.e., less than 4.0 mm, than that necessary for more rigid IOLs, i.e., 5.5 to 7.0 mm. A larger incision is necessary for more rigid IOL implants because the lens must be inserted through an incision in the cornea slightly larger than the diameter of the inflexible IOL optic portion. Accordingly, more rigid IOL implants have become less popular in the market since larger incisions have been found to be associated with an increased incidence of postoperative complications, such as induced astigmatism.

[0004] With recent advances in small-incision cataract surgery, increased emphasis has been placed on developing soft, foldable materials suitable for use in the manufacture of IOL implants. In general, the materials of current commercial IOLs fall into one of three categories: silicone, hydrophilic acrylic and hydrophobic acrylic.

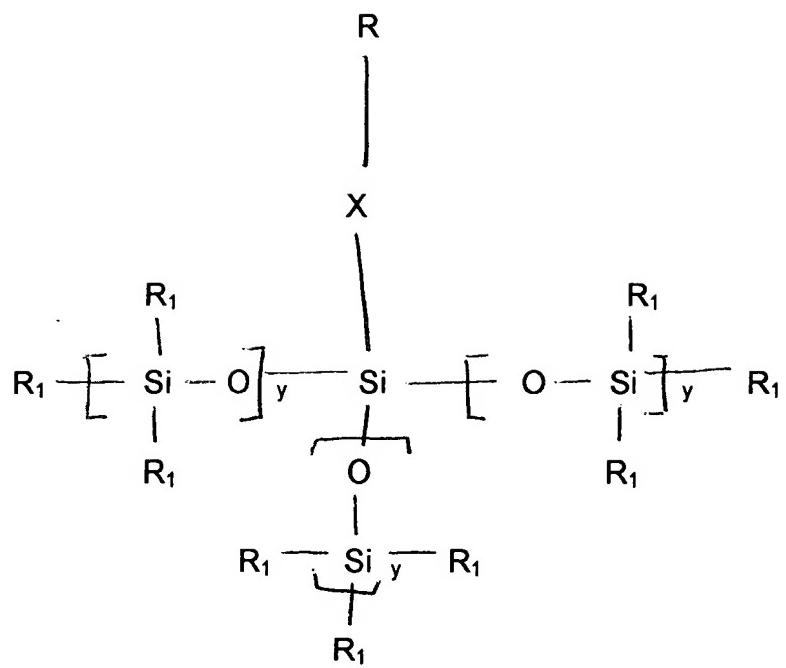
[0005] In general, high water content, i.e., 15 percent or greater water content by volume, hydrophilic acrylic materials or “hydrogels,” have relatively low refractive indexes, making them less desirable than other materials with respect to minimal incision size. Low refractive index materials require a thicker IOL optic portion to achieve a given refractive power. Silicone materials may have a higher refractive index than high-water content hydrogels, but tend to unfold explosively after being placed in the eye in a folded position. Explosive unfolding can potentially damage the corneal endothelium and/or rupture the natural lens capsule and associated zonules. Low glass transition temperature hydrophobic acrylic materials are desirable because they typically have a high refractive index and unfold more slowly and more controllably than silicone materials. Unfortunately, low glass transition temperature hydrophobic acrylic materials, which contain little or no water initially, may absorb pockets of water *in vivo* causing light reflections or “glistenings.” Furthermore, it may be difficult to achieve ideal folding and unfolding characteristics due to the temperature sensitivity of some hydrophobic acrylic polymers.

[0006] Because of the noted shortcomings of current polymeric materials available for use in the manufacture of ophthalmic devices such as IOLs, there is a need for stable, biocompatible polymeric materials having desirable physical characteristics.

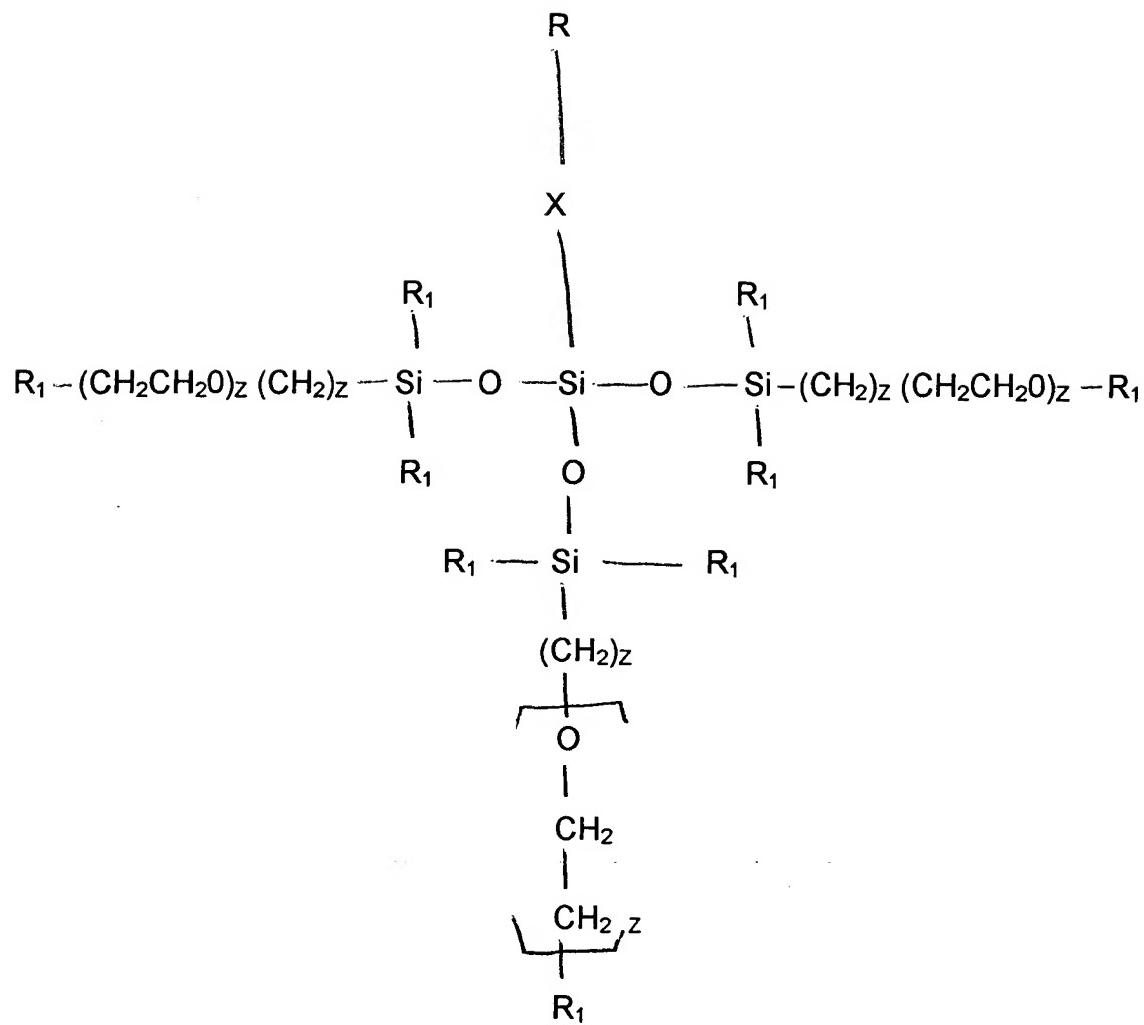
Summary of the Invention:

[0007] Soft, foldable, relatively high refractive index, polymeric compositions of the present invention are synthesized through the polymerization of one or more siloxysilane monomers or alternatively through the copolymerization of one or more siloxysilane monomers with one or more aromatic or non-aromatic non-siloxy based monomers, hydrophilic monomers or hydrophobic monomers. Polymeric compositions of the present invention are gas permeable, transparent, relatively high in strength for durability during surgical manipulation and relatively high in refractive index. The subject polymeric compositions are particularly well suited for use in the manufacture of ophthalmic devices such as but not limited to intraocular lens (IOL) implants, contact lenses, keratoprostheses, corneal rings, corneal inlays and the like.

[0008] Preferred siloxysilane monomers for use in preparing the polymeric compositions of present invention are represented by the structures of Formula 1 and Formula 2 below:



Formula 1



Formula 2

wherein R is a polymerizable group; X is selected from the group consisting of C₁₋₁₀ alkyl, C₁₋₁₀ alkyloxy, C₆₋₃₆ aryl and C₆₋₃₆ aryloxy; and the R₁ groups may be the same or different selected from the group consisting of C₁₋₁₀ alkyl, C₁₋₂₀ cycloalkyl, C₆₋₃₆ aryl, C₆₋₃₆ aryl ether, C₆₋₃₆ heterocycle, C₆₋₃₆ heterocycle with one or more substituents, C₁₋₁₀ alkyl ether and C₆₋₃₆ aryloxy; y may be the same or different non-negative integer less than 101; and z may be the same or different non-negative integer less than 20.

[0009] Accordingly, it is an object of the present invention to provide a transparent, biocompatible polymeric composition having desirable physical characteristics for use in the manufacture of ophthalmic devices.

[0010] Another object of the present invention is to provide a polymeric composition having a relatively high refractive index.

[0011] Another object of the present invention is to provide a polymeric composition suitable for use in the manufacture of an ophthalmic implant.

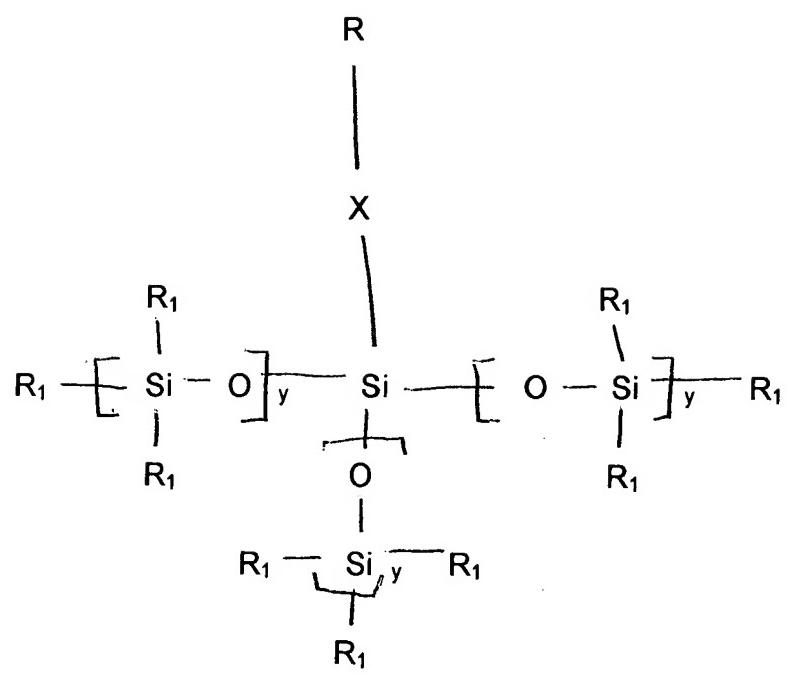
[0012] Another object of the present invention is to provide a polymeric composition that is relatively flexible with good clarity.

[0013] Still another object of the present invention is to provide a polymeric composition that is relatively simple to produce.

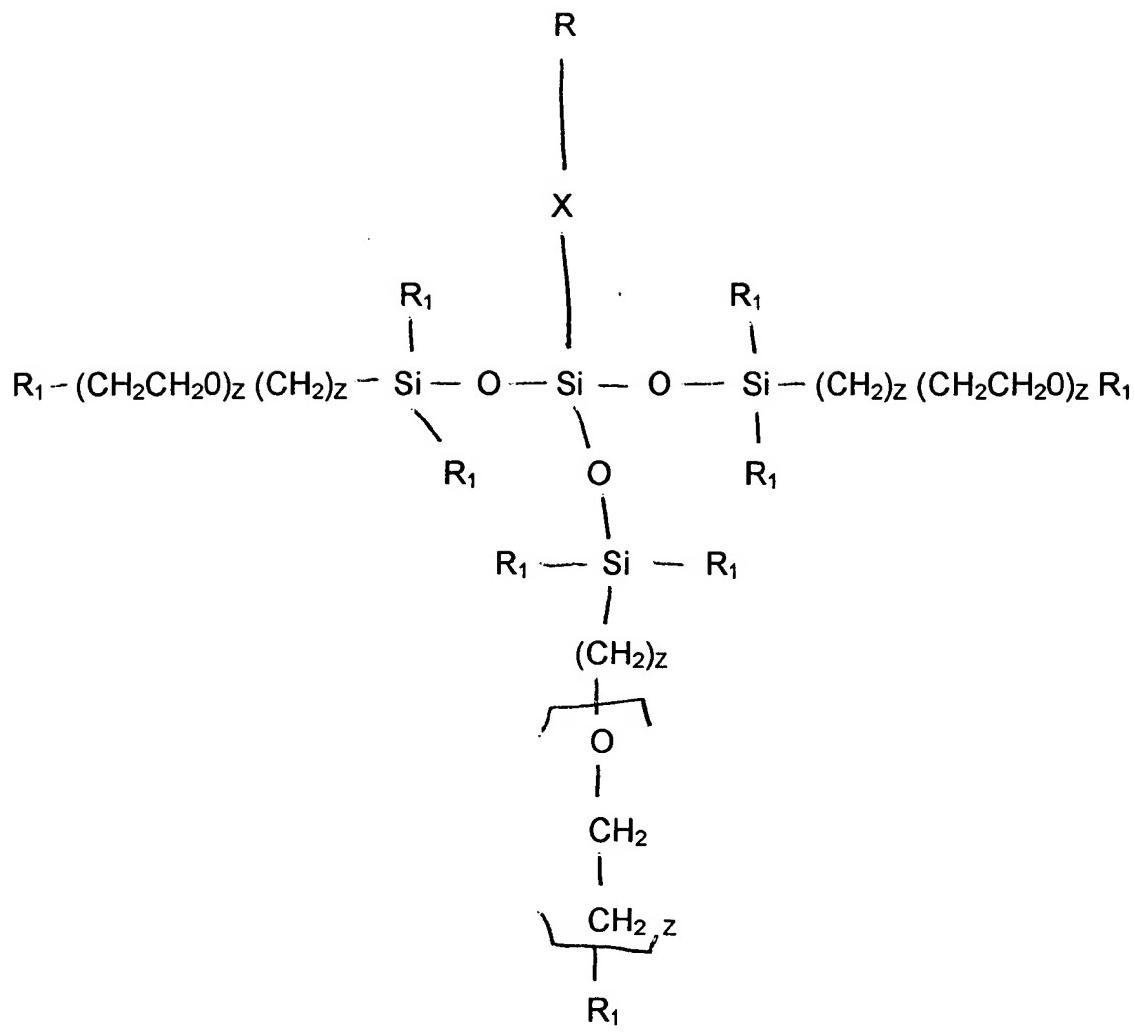
[0014] These and other objectives and advantages of the present invention, some of which are specifically described and others that are not, will become apparent from the detailed description and claims that follow.

Detailed Description of the Invention:

[0015] The present invention relates to siloxysilane monomers and the use of such monomers to produce biocompatible polymeric compositions having desirable physical properties for use in the manufacture of ophthalmic devices. The siloxysilane monomers of the present invention are represented generally by Formula 1 and Formula 2 below,



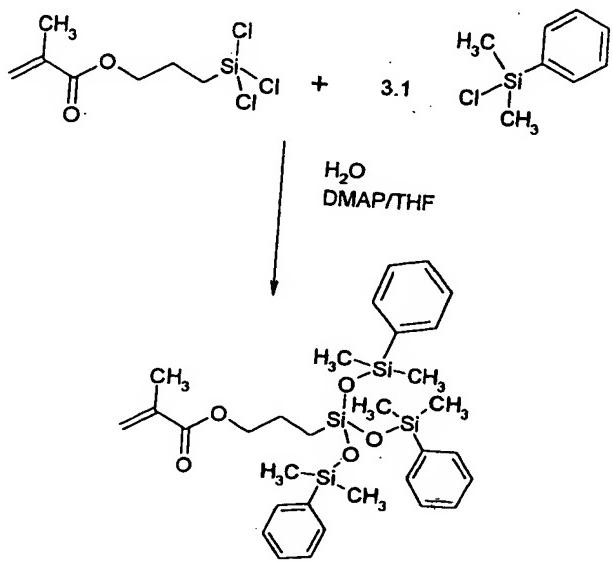
Formula 1



Formula 2

wherein R is a polymerizable group selected from the group consisting of methacrylate, acrylate, acrylamido, methacrylamido, styryl, itaconate, fumaroyl, vinyl, vinyloxy, vinyl carbamate and vinyl carbonate; X is selected from the group consisting of C₁₋₁₀ alkyl such as for example but not limited to methyl, propyl or heptyl, C₁₋₁₀ alkyloxy such as for example but not limited to ethyloxy, butyloxy or octyloxy, C₆₋₃₆ aryl such as for example but not limited to phenyl or naphthyl and C₆₋₃₆ aryloxy such as for example but not limited to phenoxy or naphthoxy; the R₁ groups may be the same or different selected from the group consisting of C₁₋₁₀ alkyl such as for example but not limited to methyl, propyl or pentyl but preferably propyl for increased stability, C₁₋₂₀ cycloalkyl such as for example but not limited to cyclohexyl or cycloheptyl, C₆₋₃₆ aryl such as for example but not limited to phenyl or naphthyl, C₆₋₃₆ aryl ether such as for example but not limited to phenyl ether or naphthyl ether, C₆₋₃₆ heterocycle such as for example but not limited to pyridine, quinoline, furan or thiophene but preferably pyridine to increase refractive index, C₆₋₃₆ heterocycle such as those described above with one or more substituents such as for example but not limited to chlorine, fluorine, amine, amide, ketone or C₁₋₃ alkyl such as for example methyl or propyl, C₆₋₃₆ aryloxy such as for example but not limited to phenoxy or naphthoxy and C₁₋₁₀ alkyl ethers such as for example methyl ether or propyl ether; y may be the same or different non-negative integer less than 101; and z may be the same or different non-negative integer less than 20.

[0016] Siloxasilane monomers of the present invention represented by Formula 1 and Formula 2 above, may be synthesized through a co-hydrolysis reaction with an acid scavenger as illustrated in Scheme 1 below.



Scheme 1

[0017] As illustrated in Scheme co-hydrolysis of 1, 3-methacryloyloxypropylchlorosilane with chlorophenyldimethylsilane using N,N-dimethylaminopyridine (DMAP) as an acid scavenger produces 3-methacryloyloxypropyltris(phenyldimethylsiloxy)silane.

[0018] Examples not intended to be limiting of siloxysilane monomers of the present invention produced as described above include for example but are not limited to m-vinylbenzyltris(trimethylsiloxy)silane, p-vinylbenzyltris(trimethylsiloxy)silane, m-vinylbenzyltris(dimethylphenylsiloxy)silane, p-vinylbenzyltris(dimethylphenylsiloxy)silane, 3-methacryloyloxypropyltris(triphenylsiloxy)silane, 3-(triphenylsilyl)propyl vinyl ether, 3,3-diphenylpropyl maleimide, 2-bromobenzyl-4-ethenylphenylether, (3-phenyldimethylsilylpropyl)-4-ethenylphenylether and 3-acryloyloxypropyl-1,1-diphenyl-(2-naphthyl)silane.

[0019] Although one or more siloxysilane monomers of the present invention may be polymerized or copolymerized to form crosslinked three-dimensional networks, one or more crosslinking agents may be added thereto in quantities less than 10 percent weight per volume (W/V) if desired prior to polymerization or copolymerization thereof.

[0020] Examples of suitable crosslinking agents include but are not limited to diacrylates and dimethacrylates of triethylene glycol, butylene glycol, neopentyl glycol, ethylene glycol, hexane-1,6-diol and thio-diethylene glycol, trimethylolpropane triacrylate, N,N'-dihydroxyethylene bisacrylamide, diallyl

一〇〇三三五二二〇

phthalate, triallyl cyanurate, divinylbenzene; ethylene glycol divinyl ether, N,N'-methylene-bis-(meth)acrylamide, sulfonated divinylbenzene and divinylsulfone.

[0021] Although not required, siloxysilane monomers within the scope of the present invention may optionally have one or more strengthening agents added thereto prior to polymerization or copolymerization, preferably in quantities of less than about 80 weight percent but more typically from about 20 to about 60 weight percent.

[0022] Examples of suitable strengthening agents are described in U.S. Patent Nos. 4,327,203, 4,355,147 and 5,270,418 each incorporated herein in its entirety by reference. Specific examples, not intended to be limiting, of such strengthening agents include cycloalkyl acrylates and methacrylates, such as for example tert-butylcyclohexyl methacrylate, isopropylcyclopentyl acrylate and tert-butylcyclohexyl acrylate.

[0023] One or more ultraviolet light absorbers may optionally be added to the subject monomers prior to polymerization or copolymerization in quantities typically less than 2 percent W/V. Suitable ultraviolet light absorbers for use in the present invention include for example but are not limited to β -(4-benzotriazoyl-3-hydroxyphenoxy)ethyl acrylate, 4-(2-acryloyloxyethoxy)-2-

hydroxybenzophenone, 4-methacryloyloxy-2-hydroxybenzophenone, 2-(2'-methacryloyloxy-5'-methylphenyl)benzotriazole, 2-(2'-hydroxy-5'-methacryloyloxyethylphenyl)-2H-benzotriazole, 2-[3'-tert-butyl-2'-hydroxy-5'-(3"-methacryloyloxypropyl)phenyl]-5-chlorobenzotriazole, 2-[3'-tert-butyl-5'-(3"-dimethylvinylsilylpropoxy)-2'-hydroxyphenyl]-5-methoxybenzotriazole, 2-(3'-allyl-2'-hydroxy-5'-methylphenyl)benzotriazole, 2-[3'-tert-butyl-2'-hydroxy-5'-(3"-methacryloyloxypropoxy)phenyl]-5-methoxybenzotriazole, and 2-[3'-tert-butyl-2'-hydroxy-5'-(3"-methacryloyloxypropoxy)phenyl]-5-chlorobenzotriazole wherein β-(4-benzotriazoyl-3-hydroxyphenoxy)ethyl acrylate is the preferred ultraviolet light absorber.

[0024] The siloxysilane monomers of the present invention produced as described above may be polymerized alone or copolymerized with other monomers. The subject siloxysilane monomers may be copolymerized with one or more aromatic or non-aromatic non-siloxy-based monomers, hydrophobic monomers, hydrophilic monomers or a combination thereof to produce polymeric compositions of the present invention.

TECHNICAL FIELD

[0025] Examples of aromatic and non-aromatic non-siloxy-based monomers useful for copolymerization with one or more siloxysilane monomers of the present invention include for example but are not limited to 2-phenyloxyethyl methacrylate, 3,3-diphenylpropyl methacrylate, glyceryl methacrylate, 3-phenylpropyl acrylate, N,N-dimethylacrylamide, methyl methacrylate, 2-(1-naphthylethyl methacrylate) and 2-(2-naphthylethyl methacrylate) but preferably 2-(1-naphthylethyl methacrylate) for increased refractive index.

[0026] Examples of hydrophobic monomers useful for copolymerization with one or more siloxysilane monomers of the present invention include for example but are not limited to 2-ethylhexyl methacrylate, 3-methacryloyloxypropyldiphenylmethysilane and 2-phenyloxyethyl methacrylate but preferably 3-methacryloyloxypropyldiphenylmethysilane for increased refractive index.

[0027] Examples of hydrophilic monomers useful for copolymerization with one or more siloxysilane monomers of the present invention include for example but are not limited to N,N-dimethylacrylamide and N-methylacrylamide but preferably N,N-dimethylacrylamide for increased hydrophilicity.

[0028] The physical and mechanical properties of copolymers produced from siloxysilane monomers of the present invention are set forth below in

Table 1 and Chart 1.

TABLE 1

Mechanical and physical property results for films based on 3-(3-methacryloyloxypropyl)-1,1,1-triphenyl-3,3-dimethyldisiloxane (MPTDS) or the acrylate (APTDS).

Composition	W/W %	R.I.	Mod (g/mm ²)	Tear (g/mm)	% H ₂ O
MPTDS/Dar	100/0.5	1.54			0
MPTDS/DMA/Eg/ Dar/Hex	54/40/3.2/2.2/20	1.49	1703	35	28
	56/42/.4/1.5/20	1.46	337	54	43
	64/33/2/1/20	1.51	4333	112	23
APTDS/Dar	100/0.5	1.54			0
APTDS/DMA/Eg/ Dar/Hex	70/30/1/0.5/20	1.524	251	64	17
	60/40/1/0.5/20	1.49	78	24	30
APTDS/DMA/ Hex/Eg/Irg	65/35/20/1/0.5	1.52	121	37	19

R.I.=Refractive Index

Mod=Modulus

Eg=Egdma=Ethylene glycol dimethacrylate

DMA=Dimethylacrylamide

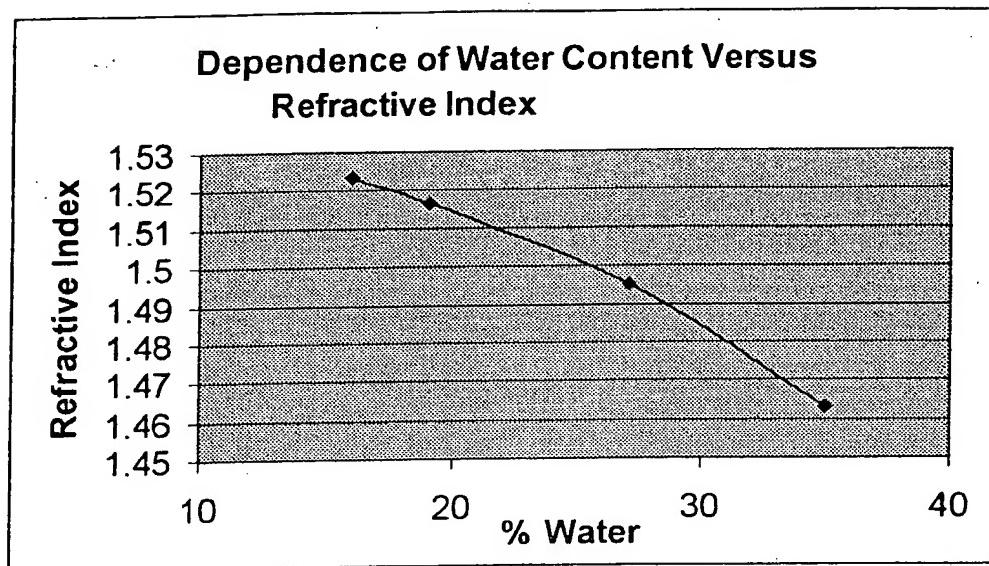
Hex=Hexanol

Dar=DarocurTM 1173 (EM Industries)

Irg=IrgacureTM 819 (Ciba-Geigy, Basel, Switzerland)

CHART 1

Dependence of water content versus refractive index for copolymers based on MPTDS and DMA.



[0029] No water content, low water content of less than 15 percent water content by volume and high water content "hydrogels" of 15 percent or higher water content by volume polymeric compositions of the present invention having ideal physical characteristics for ophthalmic device manufacture are described herein.

[0030] The polymeric compositions of the present invention are of relatively high refractive index of approximately 1.45 or greater and relatively high elongation of approximately 100 percent or greater. The polymeric compositions of the present invention with the desirable physical properties noted above are particularly useful in the manufacture of ophthalmic devices such as but not limited to relatively thin, foldable intraocular lens implants, contact lenses and corneal inlays.

[0031] IOLs having relatively thin optic portions are critical in enabling a surgeon to minimize surgical incision size. Keeping the surgical incision size to a minimum reduces intraoperative trauma and postoperative complications. A relatively thin IOL optic portion is also critical for accommodating certain anatomical locations in the eye such as the anterior chamber and the ciliary sulcus. IOLs may be placed in the anterior chamber for increasing visual acuity in either aphakic or phakic eyes, or placed in the ciliary sulcus for increasing visual acuity in phakic eyes.

)

TODD T. HEDDERICK

[0032] The polymeric compositions of the present invention have the flexibility required to allow implants manufactured from the same to be folded or deformed for insertion into an eye through the smallest possible surgical incision, i.e., 3.5 mm or smaller. It is unexpected that the subject polymeric compositions could possess the ideal physical properties described herein. The ideal physical properties of the subject polymeric compositions are unexpected since high refractive index monomers typically lend to polymers with increased crystallinity and decreased clarity, which is not true in the case of the subject polymeric compositions.

[0033] The subject siloxysilane monomers and polymeric compositions produced therefrom are described in still greater detail in the examples that follow.

EXAMPLE 1: Synthesis of MPTDS

[0034] To a 1000 ml one-neck round bottom flask fitted with a magnetic stirrer, condenser, heating mantle and nitrogen blanket, was added 500 ml CHCl₃, 18.2 grams (149 mmol) of dimethylaminopyridine (DMAP), 37.6 grams (135.9 mmol) of triphenylsilanol and 30.0 grams (135.9 mmol) of 3-methacryloyloxypropyldimethylchlorosilane.

The contents of the flask were refluxed for 72 hours and then allowed to cool to room temperature. The organics were washed twice in 500 ml 2N HCl, then dried over magnesium sulfate and flashed to an oil. After column chromatography on silica gel eluting with 80.0% heptane and 20.0% CH₂Cl₂, the product was isolated. The chromatography was monitored by thin layer chromatography (TLC) plates.

Example 2:

[0035] To 64 parts of MPTDS was added 33 parts of dimethylacrylamide, 20 parts of hexanol, 2 parts of ethyleneglycol dimethacrylate and 1.0% of Irgacure™ 819 as the UV photoinitiator and 0.25% of a commercial triazole UV blocker (Aldrich Chemical Co). The clear solution was sandwiched between two silanized glass plates using metal gaskets and exposed to UV radiation for two hours. The resultant films were released and extracted in isopropanol (IPA) for four hours, followed by air-drying and a 30 mm vacuum to remove the IPA. The resultant film was hydrated at room temperature overnight in borate buffered

saline. The clear tack-free films possessed a modulus of 4333 g/mm², a tear strength of 112 g/mm, a water content of 23% and a refractive index of 1.51.

Example 3:

[0036] To 70 parts of APTDS was added 30 parts of dimethylacrylamide, 20 parts of hexanol, 1 part of ethyleneglycol dimethacrylate and 0.5% of IrgacureTM 819 as the UV photoinitiator and 0.25% of a commercial triazole UV blocker (Aldrich Chem. Co). The clear solution was sandwiched between two silanized glass plates using metal gaskets and exposed to UV radiation for two hours. The resultant films were released and extracted in IPA for four hours, followed by air-drying and a 30 mm vacuum to remove the IPA. The resultant film was hydrated at room temperature overnight in borate buffered saline. The clear tack-free films possessed a modulus of 251 g/mm², a tear strength of 64 g/mm, a water content of 17% and a refractive index of 1.52.

Example 4:

[0037] To 70 parts of APTDS was added 10 parts of dimethylacrylamide, 20 parts of hexanol, 1 part of ethyleneglycol dimethacrylate and 0.5% of IrgacureTM 819 as the UV photoinitiator and 0.25% of a commercial triazole UV blocker (Aldrich Chem. Co). The clear solution was sandwiched between two silanized glass plates using metal gaskets and exposed to UV radiation for two hours. The resultant films were released and extracted in IPA for four hours, followed by air-drying and a 30 mm vacuum to remove the IPA. The resultant film was hydrated at room temperature overnight in borate buffered saline. The clear tack-free films possessed a water content of 10% and a refractive index of 1.53.

[0038] The siloxysilane monomers of the present invention may be readily cured in cast shapes by one or more conventional methods. Such methods include for example but are not limited to ultraviolet light (UV) polymerization, visible light polymerization, microwave polymerization, thermal polymerization, free radical polymerization, living radical polymerization or combinations thereof. Metallocene catalysts may also be used in certain instances.

[0039] One or more suitable free radical thermal polymerization initiators may be added to the monomers of the present invention. Examples of such initiators include but are not limited to organic peroxides, such as acetyl peroxide, lauroyl peroxide, decanoyl peroxide, stearoyl peroxide, benzoyl peroxide, tert-butyl peroxy pivalate, peroxy dicarbonate, and the like. Preferably such an initiator is employed in a concentration of approximately 0.01 to 1 percent by weight of the total monomer mixture.

[0040] Representative UV initiators include those known in the field such as for example but not limited to benzoin methyl ether, benzoin ethyl ether, DarocurTM 1173, 1164, 2273, 1116, 2959, 3331 (EM Industries) and IrgacurTM 651 and 184 (Ciba-Geigy, Basel, Switzerland).

[0041] Ophthalmic devices such as but not limited to IOLs made of the polymeric compositions of the present invention can be of any suitable design or form. For example, ophthalmic devices such as IOLs typically comprise an optic portion and one or more haptic portions. Once implanted within an eye, the IOL optic portion reflects light onto the retina of the eye and the permanently attached haptic portions hold the optic portion in proper alignment within the eye. The haptic portions may be integrally formed with the optic portion in a one-piece

design or attached by staking, adhesives or other methods known to those skilled in the art in a multipiece design.

[0042] The subject ophthalmic devices, such as for example IOLs, may be manufactured to have an optic portion and haptic portions made of the same or differing materials. Preferably, in accordance with the present invention, both the optic portion and the haptic portions of the IOL are made of the same polymeric composition of the present invention. Alternatively however, the IOL optic portion and haptic portions may be manufactured from different materials and/or different formulations of the polymeric compositions of the present invention, such as described in detail in U.S. Patent Numbers 5,217,491 and 5,326,506, each incorporated herein in its entirety by reference. Once the particular material or materials are selected, the same is either cast in molds of the desired form and cured, or cast in the form of rods and cured. If cast in the form of rods, the rods while in a dry state are machined or lathed into disks. The resultant disks may then be machined or lathed into IOLs or other ophthalmic devices. The IOLs or other ophthalmic devices whether molded or machined/lathed are then cleaned, polished, hydrated, packaged and sterilized by customary methods known to those skilled in the art.

[0043] In addition to IOLs, the polymeric compositions of the present invention are also suitable for use as other ophthalmic devices such as but not limited to contact lenses, keratoprostheses, capsular bag extension rings, corneal inlays, corneal rings and like devices.

[0044] IOLs and like ophthalmic devices manufactured using the unique polymeric compositions produced from the unique siloxysilane monomers of the present invention are used as customary in the field of ophthalmology. For example, in a surgical procedure, an incision is placed in the cornea of an eye. Most commonly through the corneal incision the natural lens of the eye is removed (aphakic application) such as in the case of a cataractous natural lens. An IOL or the like is then inserted into the anterior chamber, posterior chamber or lens capsule of the eye prior to closing the incision. However, the ophthalmic devices of the subject invention may be used in accordance with other surgical procedures known to those skilled in the field of ophthalmology.

[0045] While there is shown and described herein certain siloxysilane monomers and polymeric compositions of the present invention, it will be manifest to those skilled in the art that various modifications may be made without departing from the spirit and scope of the underlying inventive concept

and that the same is not limited to particular structures herein shown and described except insofar as indicated by the scope of the appended claims.

二〇〇三六三五 二〇〇一